Epidural auditory event-related potentials in the rat to frequency and duration deviants: evidence of mismatch negativity?

Tamo Nakamura¹,²,³,⁴*, Patricia T. Michie¹,²,³,⁴, William R. Fulham²,³,⁴,⁵, Juanita Todd¹,²,³,⁴, Timothy W. Budd¹,²,³,⁴, Ulrich Schall²,³,⁴,⁵, Michael Hunter¹,² and Deborah M. Hodgson¹,²,³,⁴

INTRODUCTION

Reduced amplitude of the brain event-related potential (ERP), mismatch negativity (MMN), has been a consistent finding in patients with a diagnosis of a schizophrenia spectrum disorder (Michie, 2001) with a recent meta-analysis (Umbricht and Krljes, 2005) reporting an overall effect size of 0.99. In humans, MMN is observed in response to the presentation of rare oddball sounds that deviate from an otherwise regular pattern of frequent background standard sounds. While the primate and cat auditory cortex (AC) exhibit MMN-like activity, it is unclear whether the rodent AC produces a deviant response that reflects deviance detection in a background of regularities evident in recent auditory stimulus history or differential adaptation of neuronal responses due to rarity of the deviant sound. We examined whether MMN-like activity occurs in epidural AC potentials in awake and anesthetized rats to high and low frequency and long and short duration deviant sounds. ERPs to deviants were compared with ERPs to common standards and also with ERPs to deviants when interspersed with many different standards to control for background regularity effects. High frequency (HF) and long duration deviant ERPs in the awake rat showed evidence of deviance detection, consisting of negative displacements of the deviant ERP relative to ERPs to both common standards and deviants with many standards. The HF deviant MMN-like response was also sensitive to the extent of regularity in recent acoustic stimulation. Anesthesia in contrast resulted in positive displacements of deviant ERPs. Our results suggest that epidural MMN-like potentials to HF sounds in awake rats encode deviance in an analogous manner to the human MMN, laying the foundation for animal models of disorders characterized by disrupted MMN generation, such as schizophrenia.

Keywords: mismatch negativity, deviance detection, adaptation, epidural, rat

The capacity of the human brain to detect deviance in the acoustic environment pre-attentively is reflected in a brain event-related potential (ERP), mismatch negativity (MMN). MMN is observed in response to the presentation of rare oddball sounds that deviate from an otherwise regular pattern of frequent background standard sounds. While the primate and cat auditory cortex (AC) exhibit MMN-like activity, it is unclear whether the rodent AC produces a deviant response that reflects deviance detection in a background of regularities evident in recent auditory stimulus history or differential adaptation of neuronal responses due to rarity of the deviant sound. We examined whether MMN-like activity occurs in epidural AC potentials in awake and anesthetized rats to high and low frequency and long and short duration deviant sounds. ERPs to deviants were compared with ERPs to common standards and also with ERPs to deviants when interspersed with many different standards to control for background regularity effects. High frequency (HF) and long duration deviant ERPs in the awake rat showed evidence of deviance detection, consisting of negative displacements of the deviant ERP relative to ERPs to both common standards and deviants with many standards. The HF deviant MMN-like response was also sensitive to the extent of regularity in recent acoustic stimulation. Anesthesia in contrast resulted in positive displacements of deviant ERPs. Our results suggest that epidural MMN-like potentials to HF sounds in awake rats encode deviance in an analogous manner to the human MMN, laying the foundation for animal models of disorders characterized by disrupted MMN generation, such as schizophrenia.
Garagnani and Pulvermüller (2011) point out that each emphasize "the importance of short-term mechanisms acting upon, or being driven by, the most recent sensory input" (p. 170). An alternate view of MMN that offers a more cognitive level of explanation is that proposed by Näätänen et al. (2005) that MMN results from an automatic comparison process that detects a discrepancy between a novel event and the representation of the regularity of recent stimulation retained in sensory memory.

There is increasing interest in identifying MMN-like activity in rodents in order to advance research into the neurophysiological and neurochemical mechanisms underpinning MMN generation and provide opportunities for translational MMN research such as the development of animal models of schizophrenia (Bickel and Javitt, 2009). However, an integration of previous MMN research in rats is difficult due to methodological differences between studies. These include whether MMN-like activity is measured using single/multiunit activity (MUA) and evoked local field potentials (eLFPs; von der Behrens et al., 2009; Farley et al., 2010) or from epidural sites (see Table 1), and whether controls for the physical characteristics of standard and deviant stimuli and recent stimulus history have been implemented. Similarly, the use of anesthetics during recordings makes interpretation of results problematic since anesthetics alter the physiological properties of neural elements underlying MMN activity (Roper et al., 2009). Only two of the nine previous MMN studies using epidural recordings in the rat (see Table 1) used awake (unanesthetized) animals.

The aim of the present study is to provide a comprehensive assessment of epidural potentials to frequency and duration oddball deviants in the awake unrestrained rat as well as under anesthesia and to determine whether these responses exhibit an MMN-like pattern under appropriate control conditions.

Bearing in mind that MMN is an arithmetic comparison of ERPs to rare deviant and a frequent standard sounds, a major methodological concern for rodent MMN studies is to ensure that the design allows a clear distinction between at least two explanations of why the deviant response is different, namely, a differential adaptation explanation vs. an explanation based on deviant sound violating regularities in recent stimulus history. Similar concerns have been raised with respect to stimulus-specific adaptation (SSA) phenomena evident in MUA and eLFP recordings from auditory cortex (Ulanovsky et al., 2003; Nelken and Ulanovsky, 2007; Taaseh et al., 2011). SSA is the specific decrease in the response to a frequent standard stimulus, which does not generalize to a different rare deviant stimulus. Although the term SSA emphasizes the adaptation of neural responses to repetition of sounds, as noted by Taaseh et al. (2011), a key aspect of SSA in the auditory system is the production of a large response to a rare deviant sound, that could be due either to the fact that the response to the deviant is not adapted because of its rare occurrence, that is, differential adaptation due to the rarity of the deviant, or because the deviant represents a change relative to the regularity created by repeating the standard sound, that is, deviance detection. Similar alternate possibilities are relevant to the interpretation of MMN-like activity in evoked epidural recordings in the rat.

A common solution implemented in previous rat studies that attempts to distinguish rarity from deviance detection explanations of MMN-like responses is inclusion of the deviant-alone condition (see Table 1) in the design where intervals between successive deviants are the same as in the oddball sequence but no standards are presented (i.e., silence intervenes between successive deviants). However, while the deviant-alone condition controls for the interval between successive deviants (one index of rarity), it does not control for contributions from the deviant interrupting regularity in background stimulation. Therefore, a control condition is required where multiple different tones intervene between successive deviants so that there is no regularity in recent stimulation present. The “many standards” control condition first employed by Jacobsen and Schröger (2001) in the human literature meets these requirements and also controls for rarity; the deviant is presented at the same probability in the many-standards sequence as in the oddball sequence with constant or “common” standards. A number of animal studies have previously utilized this control condition in MUA and eLFP investigations of SSA (Ulanovsky et al., 2003; Farley et al., 2010; Taaseh et al., 2011) and in one very recent study of MMN in rat epidural recordings (Astikainen et al., 2011). An additional important issue for the interpretation of differences between the deviant and standard response in rodent epidural recordings is that any observed differences cannot be explained solely by the physical differences between sounds. This requires a design in which the roles of standards and deviants are reversed in oddball sequences (often called a flip-flop design) so standard and deviant ERPs are elicited by stimuli with identical physical characteristics. The many-standards control also allows a comparison between ERPs to oddball deviants and to sounds (referred to here as control deviants) with identical physical characteristics and probability of occurrence.

MATERIALS AND METHODS
SUBJECTS, SURGICAL PROCEDURES, AND ELECTROPHYSIOLOGICAL RECORDINGS
The experiments were performed on seven Wistar rats (six males). The surgery was performed when the male animals were on average 182 days old (144–216 days old) and the female rat was 201 days old. The average weight of the male animals was 566.4 g (505.1–603.9 g) on the day of surgery and the female rat 320.7 g. This study was approved by the University of Newcastle Animal Care and Ethics Committee (A-2009-108) and all experiments conformed to the relevant regulatory standards.

Animals were anesthetized with fentanyl (300 μg/kg i.p.) and medetomidine (300 μg/kg i.p.), and/or isoflurane and the rat placed on a heating pad during surgery. A battery operated biotelemetric radiotransmitter (model # TA11CA-F40, Data Sciences International, St. Paul, MN, USA) was implanted in the peritoneal cavity. Insulated biopotential leads from the transmitter were passed subcutaneously to the base of the skull. The skin over the skull was exposed and two small burr holes were drilled in the skull, one hole for the active electrode over the right auditory cortex (4.5 mm posterior to the bregma and 3.5 mm lateral to the midline) and the other for the reference electrode in the left hemisphere (2 mm posterior to the lambda and 2 mm lateral to the midline). These locations are based on previous research demonstrating MMN-like epidural responses in the rat (Tikhonravov et al., 2008). The leads were fixed with dental acrylic. Carprofen
Table 1 | Summary of previously published papers on epidural mismatch negativity (MMN) potentials in rats showing details of animal state, location of recording sites, deviant feature, design control details, polarity of the MMN, and latency window of the effect.

<table>
<thead>
<tr>
<th>Author</th>
<th>State: awake vs. anesthesia</th>
<th>Location of active and reference sensors</th>
<th>Deviant feature</th>
<th>Design controls</th>
<th>Polarity of MMN response</th>
<th>Window of effect (ms)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Astikainen et al. (2006)</td>
<td>Urethane</td>
<td>Active sensor – same as reported in Ruusuvirta et al. (1998). Reference – over the nasal bone.</td>
<td>Frequency, frequency and intensity conjunctions</td>
<td>Flip-flop design; frequency and intensity conjunctions controlled for adaptation effects</td>
<td>+ve</td>
<td>76–108</td>
</tr>
<tr>
<td>Astikainen et al. (2011)</td>
<td>Urethane</td>
<td>Active sensor positioned on the basis of response to tone stimuli within a 4-mm x 4-mm exposed region of dura over the auditory cortex in the left hemisphere, 4.5–6.5 mm posterior to bregma and 3.0–5.0 mm ventral to bregma. Reference – positioned over the right side of the brain above the cerebellum (AP −11.0 mm, ML 3.0 mm). Ground – positioned over the right side of the brain above the frontal cortex (AP +4.0 mm, ML 3.0 mm).</td>
<td>Ascending and descending frequency</td>
<td>Many-standards control condition</td>
<td>+ve but significant only for ascending frequency deviants</td>
<td>60–100</td>
</tr>
<tr>
<td>Eriksson and Villa (2005)</td>
<td>Awake; ketamine and xylazine hydrochloride</td>
<td>Multi-electrode arrays were positioned bilaterally in the lower cortical layers (IV–VI) in the core auditory regions of the temporal cortex. Reference – an epidural electrode was positioned in the anterior part of the skull.</td>
<td>Synthetic vowels with a different fundamental and/or formant frequencies</td>
<td>Flip-flop design; deviant-alone condition</td>
<td>No MMN</td>
<td>N/A</td>
</tr>
<tr>
<td>Lazar and Metherate (2003)</td>
<td>Urethane–xylazine</td>
<td>Active sensor over the right auditory cortex, slightly posterior to the 10-kHz frequency representation in the primary auditory cortex in layer IV. Reference – skull screw on the right cerebellar cortex.</td>
<td>Frequency</td>
<td>No flip-flop design; condition which approximated a deviant-alone condition</td>
<td>No MMN</td>
<td>N/A</td>
</tr>
<tr>
<td>Roger et al. (2009)</td>
<td>Awake</td>
<td>Active sensors – two on parietal cortices (bregma AP −4.0 mm, L +2.5 mm). Reference – bregma AP 4.5 mm, L 1.6 mm.</td>
<td>Shorter duration</td>
<td>No flip-flop</td>
<td>−ve</td>
<td>25–75 after deviant off-set</td>
</tr>
<tr>
<td>Ruusuvirta et al. (1998)</td>
<td>Urethane–xylazine</td>
<td>Active sensor positioned on the basis of response to click stimuli within a 5-mm x 5-mm exposed region with the rostral edge, 3 mm posterior to bregma and the medial edge 5 mm lateral to the midline. Reference – a skull screw on the right cerebellar cortex.</td>
<td>Frequency</td>
<td>Flip-flop design; deviant-alone condition</td>
<td>+ve</td>
<td>63–196</td>
</tr>
<tr>
<td>Ruusuvirta et al. (2007)</td>
<td>Urethane</td>
<td>Active sensor – bregma AP −5.0 mm, L 7.0 mm. Reference – lambda AP 1.0 mm, R 1.0 mm.</td>
<td>Melodic contour</td>
<td>Flip-flop design</td>
<td>Polarity varied across animals</td>
<td>106–136</td>
</tr>
</tbody>
</table>

(Continued)
(5 mg/kg s.c.) and buprenorphine (0.01 mg/kg s.c.) were administered pre-operatively as analgesics. The animals were allowed to recover for at least 6 days after surgery before the first ERP recordings in the awake state.

Event-related potentials were recorded in a plastic experimental chamber with sides covered with grounded copper mesh using custom EEG software written in LabVIEW (version 8.2.1). The experimental chamber was located inside a Faraday cage. The rat was placed in a partition (internal dimensions: length 23.5 cm, width 12.0 cm, height 24.0 cm) within the experimental chamber. For recordings in the anesthetized state, the animal was placed on its side on the bedding lengthwise in the partition. Three channels of data were continuously digitized (1 kHz): a single EEG-channel, square wave signals generated by the PC sound card in parallel with the auditory stimulus and stimulus event codes. The bandwidth of the data acquisition system was 0.2–150 Hz and the input voltage range was ±10 mV.

SOUND GENERATION
Auditory stimuli were generated with a custom program written in Presentation (Version 14.1, Neurobehavioral Systems, Inc.), amplified, and delivered through a speaker (50 Hz–19 kHz frequency response) mounted at an approximate height of 1 m above the floor of the experimental chamber. Sound intensity was calibrated with a sound meter (Brüel & Kjær Model 2260) and varied between 96 and 105 dB SPL across locations within the chamber for the sounds in the 2- and 4.5-kHz range utilized in this study. Thresholds for rats in this range are between 35 and 45 dB SPL (Jamison, 1951; Gourevitch, 1965; Mazurek et al., 2010).

EXPERIMENTAL DESIGN, STIMULUS CHARACTERISTICS, AND STIMULUS PRESENTATION
There were three types of stimulus sequences (see Figure 1A). There were two oddball sequences consisting of simple invariance deviants, where the roles of the deviant and standard were reversed (flip-flop conditions) resulting in either an ascending deviant sequence or a descending deviant sequence. The third condition was a many-standards control sequence in which stimuli equivalent to the deviants of the oddball sequences were presented at the same probability as in the oddball sequences but interspersed with other varying sounds that precluded establishment of regularity in background sounds (Jacobsen and Schröger, 2001; Nelken and Ulanovsky, 2007). Rats were tested on one frequency and one duration block within each test session in counterbalanced order across rats with a 5-min break between the two blocks. Each block contained 12 subblocks (3 experimental sequences repeated 4 times). Each subblock consisted of 250 tones in either an ascending deviant oddball sequence, a descending deviant oddball sequence or a control sequence.

In the ascending and descending oddball sequences (Figure 1A), 80% of the tones were standards (ST) and 20% deviants (DEV). Tones were presented in a pseudorandom order with the constraint that there was at least one ST before each DEV. In the control sequence, there were five types of tone bursts each presented with 20% probability to match the probability of the DEV in the ascending or descending oddball sequences. Tones were presented in pseudorandom order except that no tone was ever repeated. For all sequences, tones had a 10-ms rise and fall time and a stimulus onset asynchrony (SOA) of 500 ms.

For the frequency oddball blocks, two tone bursts of 100 ms duration were used: low frequency (LF) of 2500 Hz and high frequency (HF) of 3600 Hz equivalent to a normalized frequency difference (Δf) of 0.37, the largest frequency separation employed by Ulanovsky et al. (2003). In the ascending oddball sequence, the LF and HF tone bursts were the ST and DEV respectively. In the descending oddball sequence, the DEV and ST were reversed. In the many-standards control sequences, five frequencies (each of 100 ms duration) differing on a logarithmic scale were presented: 2083 Hz, 2500 (LF) Hz, 3000 Hz, 3600 (HF) Hz, and 4320 Hz. These tones were presented with a probability of 20% in a pseudorandom order, except for the constraint noted above.

For the duration oddball blocks, two durations, short duration (SD) of 50 ms and a long duration (LD) of 150 ms, were used (both 3000 Hz) based on the observation by Roger et al. (2009) that these durations resulted in robust MMN-like activity in the rat in a descending sequence. In the ascending oddball sequence, the SD and LD tones were the ST and DEV respectively. In the descending sequence, the ST and DEV were reversed. The duration control

Table 1 | Continued

<table>
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<th>Polarity of MMN response</th>
<th>Window of effect (ms)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Tikhonravov et al. (2008)</td>
<td>Pentobarbital sodium</td>
<td>Active sensor – bregma AP − 4.5 mm, R 3.5 mm. Reference – lambda AP − 2.0 mm, L 2.0 mm.</td>
<td>Frequency</td>
<td>Flip-flop design; deviant-alone condition</td>
<td>+ve</td>
<td>150–180</td>
</tr>
<tr>
<td>Tikhonravov et al. (2010)</td>
<td>Pentobarbital sodium</td>
<td>Active sensor – bregma AP − 4.5 mm, R 5.0 mm. Reference – lambda AP − 2.0 mm, L 2.0 mm.</td>
<td>Frequency</td>
<td>Flip-flop design; deviant-alone condition</td>
<td>+ve</td>
<td>91–180</td>
</tr>
</tbody>
</table>

1Flip-flop designs entail two oddball sequences with identical stimuli but where the roles of standards and deviants are reversed, e.g., high frequency deviant and low frequency standard in one sequence, and low frequency deviant and high frequency standard in the other. This design allows control of stimulus physical features in deviant minus standard difference waves. L, left from the midline, R, right from the midline.

2Active electrodes were not positioned on the dura but in lower cortical layer (IV–VI), although the reference was on the dura.
sequence consisted of five tones at 3000 Hz differing in durations on a logarithmic scale, 29 ms, 50 (SD) ms, 87 ms, 150 (LD) ms, and 260 ms.

In order to avoid the possibility of an MMN being elicited by tones at the extremes of a range for either the frequency or duration control conditions, known as the extreme sub-standard effect (Winkler et al., 1990; Jacobsen and Schröger, 2001; Jacobsen et al., 2003) that is particularly marked for duration (Jacobsen and Schröger, 2001; Jacobsen et al., 2003), the ST and DEV frequencies and durations used in the ascending and descending sequences were the second and the fourth highest frequencies or durations in the frequency and duration blocks, respectively.

Each animal underwent four recording sessions in an awake state on different days. The rat was placed in the partition of the experimental chamber with bedding for 15 min before each session to acclimatize. Each session lasted approximately 65 min. The rat did not have access to food or water during the session but was free to explore during the recordings. For recordings in the anesthetized state, the animal was placed in the partition (15 min) after it was anesthetized with fentanyl (300 μg/kg i.p.) and medetomidine (300 μg/kg i.p.). Two recording sessions under anesthesia occurred on the same day. This study was part of a larger project that also investigated the effects of SOA on early ERP components in sessions that were of approximately 60 min duration. For five animals, the four MMN sessions in the awake state preceded the two MMN sessions under anesthesia; in one animal, the anesthesia sessions occurred after three awake sessions; and in the other, anesthesia sessions occurred after two awake sessions.

### DATA ANALYSIS

The anesthesia data in general were noisier than the awake data, partly because the EEG during anesthesia exhibited high amplitude slow wave activity that contributed to unstable pre-stimulus baselines and slow fluctuations in the post-stimulus epochs (Figure 1B) and partly because of the fewer sessions recorded under anesthesia compared to awake sessions (two vs. four sessions). The frequency spectrum of the awake EEG was maximal at low frequencies, and decreased monotonically with frequency, except for a large peak between 6 and 8 Hz (Figure 1C). In contrast, the EEG under anesthesia had a peak at 1 Hz which was four times the amplitude of the spectrum in the awake data, and no peak in the 6–8 Hz band consistent with previous reports of increased activity in the delta frequency band (0.5–4.0 Hz) in the rat with fentanyl administration (Cox et al., 1999; Haberham et al., 2000).

Data processing was performed off-line with EEG Display 6.1.5 (Fulham, 2009). For the analyses of the auditory ERPs, epochs were extracted from the continuous EEG consisting of a 50-ms prestimulus baseline and a 200-ms post-stimulus interval. An artifact rejection threshold was set independently for each rat/recording session at 5 standard deviations of the raw EEG signal amplitude relative to the pre-stimulus baseline. On average, this resulted in 3% of the trials being rejected (range 1–13%). The single female rat exhibited very large amplitude evoked responses. As all statistical comparisons were within subject comparisons, this animal’s data were scaled down by multiplying by 0.25.

The first 25 tones at the start of each tone sequence were excluded from analysis to allow for transitory effects associated with switching between different types of sequences. Although the stimulus generation paradigm incorporated a rule that every DEV must be preceded by at least one ST, preliminary analysis showed that there was virtually no MMN-like response for oddball DEVS that were preceded by only one ST. Therefore, only EEG epochs to oddball DEVS and STs preceded by at least two STs were used in the main analysis focused on determining whether an MMN is present or not. Similarly, only epochs to control DEVS preceded by at least two tones of a different type were included.

Following these pre-processing steps, epochs were averaged off-line for each animal and session separately and ERPs extracted for each of the four basic stimulus types (HF and LF in the frequency blocks, and LD and SD in the duration blocks). For the
main analysis, we extracted ERPs to each stimulus type when they were:

i. Oddball DEVs, that is, when the stimulus was the deviant in an oddball sequence,
ii. All STs, that is, when the stimulus was the standard in an oddball sequence averaged over all standards in the sequence,
iii. STs before deviants, that is, when the stimulus was the standard in an oddball sequence but averaged over only standards that occurred immediately before the deviant (this ensures equivalent S/N for STs and DEVs, Ruusuvirta et al., 1998) or iv. Control DEVs, that is, when the stimulus occurred in a control sequence.

In general, there was little difference between ERPs to all STs and ERPs to STs before deviants in oddball runs, so the results of the latter analysis are not reported here for the main MMN analysis. Two difference waveforms were also extracted in which ERPs to all STs and control DEVs were subtracted from oddball DEVs. As outlined in the results, other post-processing of oddball DEVs and STs was undertaken in addition to the main MMN analysis to explore the effects of stimulus sequence structure, for example, the number of STs preceding a deviant in oddball sequences.

Mean amplitudes were extracted over windows that captured peaks and troughs in the ERPs to the stimulus onsets of tone bursts and effects evident in contrasts of (i) oddball DEV ERPs with ST ERPs and (ii) oddball DEV ERPs with control DEV ERPs. As the latencies of ERP components differed in awake and in anesthetized data and as effects in DEV ERP contrasts differed across frequency and duration oddball sequences, windows that capture these features are described in the Section “Results.” Mean amplitudes measuring these components and effects were analyzed in general as repeated measures analyses of variance (ANOVAs), with factors appropriate for the question of interest using a significance level of 0.05, although some outcomes approaching 0.05 are reported as trends. In instances where multiple levels were compared (such as the effect on ERP amplitudes of the five stimulus frequencies/durations from the control sequences) and where sphericity was violated, Huynh–Feldt adjusted degrees of freedom were used to determine significance levels.

RESULTS

EPIDURAL ERP MORPHOLOGY IN THE AWAKE AND ANESTHETIZED RATS

Event-related potentials to the onsets of brief tone bursts recorded from an active epidural electrode located over right auditory cortex (and a more posteriorly located left hemisphere reference) in unrestrained rats exhibited distinct components over the first 200 ms (Figure 2A), although the amplitudes of these components differed according to stimulus attribute (HF, LF, LD, and SD stimuli). In general, they were characterized by a negative component peaking at approximately 29 ms (denoted as N29AW), followed by...
a positive peak at 38 ms (P38\textsubscript{AW}) and a second broad negative component with a peak latency of approximately 90 ms (N90\textsubscript{AW}).

Three mean amplitude measures were extracted over latency windows corresponding to these peaks in awake ERPs: a 4-ms window from 27 to 31 ms centered on N29\textsubscript{AW}, a 4-ms window from 37 to 41 ms around P38\textsubscript{AW}, and a 20-ms window from 80 to 100 ms around N90\textsubscript{AW}. The HF stimulus also generated an early P19\textsubscript{AW} preceding N29\textsubscript{AW} that was not evident in ERPs to the other stimuli and a discernible notch between P38\textsubscript{AW} and N90\textsubscript{AW} peaks at approximately 42 ms. The HF stimulus generated the largest N29\textsubscript{AW} and N90\textsubscript{AW} peaks while the LF stimulus generated the smallest P38\textsubscript{AW} and N90\textsubscript{AW} peaks. The effect of tone burst frequency on the amplitudes of N29\textsubscript{AW}, P38\textsubscript{AW}, and N90\textsubscript{AW} components is most clearly evident in the ERPs to the frequencies utilized in the many-standards frequency control sequence (Figure 2B). Repeated measures ANOVAs with tone burst frequency as a single repeated measures factor on N29\textsubscript{AW}, P38\textsubscript{AW}, and N90\textsubscript{AW} mean amplitude measures confirmed the frequency differences and revealed a linear increase in amplitude of each component with increasing frequency, although for P38\textsubscript{AW} and N90\textsubscript{AW}, there was evidence of a significant fourth order non-linear contribution of increasing frequency as well \[N29\textsubscript{AW}: F(1,84, 11.05) = 4.42, p = 0.041, \text{s}e\text{cond} \text{a}r\text{ound} \text{1}, \text{6} = 33.16, p = 0.001; \text{P38}\textsubscript{AW}: F(4, 24) = 4.31, p = 0.009, \text{s}e\text{cond} \text{a}r\text{ound} \text{1}, \text{6} = 9.51, p = 0.022, \text{q}uartic \text{c}on\text{tr}ast \text{a} = \text{F}(1, 6) = 8.58, p = 0.026; \text{N90}\textsubscript{AW}: F(2, 24) = 9.04, p < 0.001, \text{linear} \text{c}on\text{tr}ast \text{a} = \text{F}(1, 6) = 22.52, p = 0.003, \text{q}uartic \text{c}on\text{tr}ast \text{a} = \text{F}(1, 6) = 10.33, p = 0.018; \text{Figure 2C}].

Differing durations from the many-standards duration control sequence had little effect on the same components (Figure 2D). Despite the LD of some tone bursts, there was no evidence of offset responses in the expected latency range after stimulus offset (see Figure 2D for 29, 50, and 87 ms durations).

Event-related potentials to the onset of brief tone bursts in the anesthetized rat exhibited components that differed markedly in morphology, amplitude, and latency to the awake data (Figures 3A–C). They were characterized by small amplitude components in general consisting of an early negative peak at 17 ms, N17\textsubscript{AN} (a negative peak at 17 ms in the anesthesia data), a subsequent positive peak at 44 ms, P44\textsubscript{AN}, and a second negative peak at 67 ms, N67\textsubscript{AN}, and a second positive peak at 90 ms, P90\textsubscript{AN}.

Three mean amplitude measures were extracted over latency windows corresponding to first three peaks in onset potentials: a 4-ms window from 15 to 19 ms centered on N17\textsubscript{AN}, a 4-ms window from 42 to 46 ms around P44\textsubscript{AN}, and a 4-ms window from 65 to 69 ms around N67\textsubscript{AN}. There was no significant systematic relationship between the amplitude of onset potentials, N17\textsubscript{AN}, P44\textsubscript{AN}, and N67\textsubscript{AN}, and tone burst frequencies from the many-standards frequency control condition \[N17\textsubscript{AN}: F(4, 24) = 2.23, p = 0.096; P44\textsubscript{AN}: F(4, 24) = 1.60, p = 0.207; N67\textsubscript{AN}: F(4, 24) = 1.25, p = 0.317; \text{Figure 3B}]. There was no effect of stimulus duration on onset potentials \[N17\textsubscript{AN}: F(4, 24) = 1.30, p = 0.297; P44\textsubscript{AN}: F(4, 24) = 1.18, p = 0.345; N67\textsubscript{AN}: F(4, 24) = 1.46, p = 0.247; \text{Figure 3C}]. But in contrast to awake data, there was evidence of offset potentials consisting of negative and positive peaks approximately 28 and 36 ms following stimulus offset of the 50-, 87-, 150-, and 260-ms tone bursts (see Figure 3C for 50, 87, and 150 ms durations).
EPIDURAL ERPs TO HIGH FREQUENCY AND LOW FREQUENCY ODDBALL DEVIANTS IN AWAKE RATS

High frequency oddball DEVs when compared to HF STs (Figure 4A) produced a larger N29<sub>AW</sub> as well as a later negative shift after P38<sub>AW</sub> with maximum separation at approximately 42 ms that persisted until approximately 90 ms. The contrast between the HF oddball and HF control DEV ERPs produced a similar pattern except that the later negative separation was more marked over longer latencies. Two difference waves were derived: HF oddball DEV ERP minus HF ST ERP, and HF oddball DEV ERP minus control DEV ERP (Figure 4B). The first negative peak in the difference waves corresponds to N29<sub>AW</sub>. The second negative peak in the difference waves corresponds to Nd42<sub>AW</sub>.

FIGURE 4 | Epidural recorded ERPs in the awake rat to oddball deviant (oddball DEV), standard (ST) and control deviant (control DEV) in the frequency conditions. (A) ERPs to high frequency (HF) stimuli. N29<sub>AW</sub>, Nd42<sub>AW</sub>, and late DIFF<sub>AW</sub> are all more negative in the oddball DEV ERP (red) than in the ST (blue) and control DEV (black). The black horizontal bar depicts the latency window over which late DIFF<sub>AW</sub> was measured. (B) MMN difference waves for HF stimuli: HF oddball DEV minus HF ST (blue), which can reflect both deviance detection and adaptation effects vs. difference waves derived using control deviants, HF oddball minus HF control DEV (black). Only the oddball DEV minus ST difference wave shows similarities in terms of polarity to the HF pattern (except for the effect on N29<sub>AW</sub>). (C) ERPs to low frequency (LF) stimuli. N29<sub>AW</sub>, Nd42<sub>AW</sub>, and late DIFF<sub>AW</sub> show inconsistent differences between the oddball DEV ERP (red) relative to the LF ST (blue) and relative to the control DEV (black). (D) MMN difference waves for LF stimuli: LF oddball DEV minus LF ST (blue), difference waves derived using control deviants, LF oddball minus LF control DEV (black). Only the oddball DEV minus ST difference wave shows similarities in terms of polarity to the HF pattern (except for the effect on N29<sub>AW</sub>). (E) The mean amplitude (with SE) of N29<sub>AW</sub>, Nd42<sub>AW</sub>, and late DIFF<sub>AW</sub> measures generated by high and low frequency oddball DEVs (gray) and STs (white). (F) The mean amplitude (with SE) of N29<sub>AW</sub>, Nd42<sub>AW</sub> and late DIFF<sub>AW</sub> measures generated by high and low frequency oddball DEVs (gray) and control DEVs (white).
peak in the difference waveforms will be called Nd42AW (a negative deflection at 42 ms in the MMN difference waveforms in the awake animal). This corresponds to the notch in the negative going arm of N90AW in the raw waveforms (Figure 4A). The later negativity in the difference waveforms will be called the late DIFFAW1 (the first late difference measure in the awake animal to distinguish it from other later effects in the duration deviant oddball paradigms).

As noted earlier, LF tone bursts in general elicited smaller amplitude ERPs than HF stimuli (Figures 2A,B) emphasizing the importance in animal models of controlling for stimulus features in MMN paradigms when recording epidural potentials as well as MUs and eLFPs (Nelken and Ulanovsky, 2007). While inspection of the LF ERPs averaged across all seven animals (Figure 4C) suggest differences between LF oddball DEV compared with LF ST and LF control DEV ERPs, particularly in the interval following P38AW, the two difference waveforms created from LF oddball DEV vs. LF ST and LF control DEV respectively were of opposite polarity from 30 to 70 ms (Figure 4D) and bore no resemblance to the HF data.

In order to capture the oddball DEV effects for both HF and LF stimuli, in addition to N29AW, two additional mean amplitudes were extracted from oddball DEV, all standards, and control DEV ERPs: Nd42AW was measured over a 4-ms window from 40 to 44 ms centered near the second negative peak in difference waves, and late DIFFAW1 over a 20-ms window from 50 to 70 ms over longer latencies of the difference wave. These two measures together with N29AW were intended to capture the early and later differences evident in the HF and LF difference waveforms.

Omnibus two-way repeated measures ANOVAs were carried out on each of the ERP measures, N29AW, Nd42AW, and late DIFFAW1, with repeated measures on frequency (HF vs. LF stimuli) and stimulus type (either oddball DEV vs. ST or oddball DEV vs. control DEV). Where the interaction between stimulus frequency and type was significant, simple effect contrasts of oddball DEV vs. ST or control DEV were conducted.

For the ANOVA in which stimulus type factor contrasted oddball DEV with ST ERPs, the oddball DEV produced a negative displacement of both N29AW and Nd42AW relative to the ST [N29AW: F(1, 6) = 7.99, p = 0.03; Nd42AW: F(1, 6) = 43.46, p = 0.001]. There was no evidence of a similar effect on late DIFFAW1. N29AW was also larger (more negative) to HF than LF stimuli [F(1, 6) = 13.20, p = 0.011; Figure 4F]. Similar main effects were not evident for Nd42AW. The interaction between stimulus frequency and type was significant for all three components [N29AW: F(1, 6) = 8.93, p = 0.024; Nd42AW: F(1, 6) = 6.65, p = 0.042; late DIFFAW1: F(1, 6) = 13.66, p = 0.010]. Simple contrasts indicated that the negative displacement of the oddball DEV relative to the control DEV was significant for HF stimuli only: N29AW (t = 2.94, p = 0.026), Nd42AW (t = 2.70, p = 0.036), late DIFFAW1 (t = 2.55, p = 0.043; Figure 4F).

The outcomes from the two contrasts are quite similar – with the exception that in the oddball deviant vs. control deviant contrast only HF stimuli exhibit a larger (more negative) Nd42AW and there are more robust effects on late DIFFAW1 (compare Figures 4A–F). Therefore, it appears that ERPs to the HF oddball deviant, at least in the awake animal, reflect deviance detection relative to background context, and not solely rarity. These deviance detection effects as defined here are evident in the earliest ERP component (i.e., N29) that occurred in epidural recordings in response to frequencies across the control frequency range and therefore might be considered an effect on an exogenous component. The deviance detection effects over later latencies, the first peaking at approximately 42 ms (referred to here as Nd42AW) and the second, a slow negative displacement spanning a broad interval (late DIFFAW1) do not appear to be effects on exogenous components. There is no clear evidence of Nd42AW as a separate exogenous ERP component across the frequency range although it appears to coincide with a notch between P38AW and N90AW in ERPs to the two highest frequencies (3600 and 4320 Hz; Figure 2B). The slow negative displacement over longer latencies does not coincide with any exogenous peak. These data suggest that we have recorded MMN-like activity to HF tone bursts in the awake rat.

To support this conclusion, we also examined the temporal evolution of responses to standards and deviants to determine whether these MMN-like effects to HF tone bursts are sensitive to the short-term stimulus history of background regularity. For this analysis we determined whether the number of preceding standards had a systematic effect on oddball DEV ERPs (Figure 5A – left panel) using ANOVAs with a single repeated measures factor with five levels (1, 2, 3, 4, or 5+ STs preceding the DEV). It was found that N29AW increased in amplitude as a function of the number of preceding standards [F(4, 24) = 3.74, p = 0.017, linear contrast – F(1, 6) = 12.33, p = 0.013, cubic contrast – F(1, 6) = 7.69, p = 0.032]. Nd42AW showed a similar pattern except that the cubic contrast was not significant [F(4, 24) = 3.49, p = 0.022, linear contrast – F(1, 6) = 8.54, p = 0.027] but there was no systematic effects of short-term stimulus history on the later negativity, late DIFFAW1. The last standard in a sequence of HF standards to support this conclusion, we also examined the temporal evolution of responses to standards and deviants to determine whether these MMN-like effects to HF tone bursts are sensitive to the short-term stimulus history of background regularity. For this analysis we determined whether the number of preceding standards had a systematic effect on oddball DEV ERPs (Figure 5A – left panel) using ANOVAs with a single repeated measures factor with five levels (1, 2, 3, 4, or 5+ STs preceding the DEV). It was found that N29AW increased in amplitude as a function of the number of preceding standards [F(4, 24) = 3.74, p = 0.017, linear contrast – F(1, 6) = 12.33, p = 0.013, cubic contrast – F(1, 6) = 7.69, p = 0.032]. Nd42AW showed a similar pattern except that the cubic contrast was not significant [F(4, 24) = 3.49, p = 0.022, linear contrast – F(1, 6) = 8.54, p = 0.027] but there was no systematic effects of short-term stimulus history on the later negativity, late DIFFAW1. The last standard in a sequence of HF standards on the other hand, showed no systematic changes as a function of the number of preceding standards (Figure 5A – right panel; F-value > 0.05). Difference waveforms were created to demonstrate the increasing negative displacements of oddball deviants more clearly by subtracting the ERPs to the common standard from deviant ERPs for deviants with 1–5+ preceding standards (Figure 5B) and means plotted for each component (Figure 5C). These demonstrate that N29AW and Nd42AW show different sensitivities to local stimulus history context (Figures 5B,C): N29AW
show a monotonic increase in amplitude with 1–4 preceding standards and a decrease at 5+ whereas Nd42AW amplitude is constant over 1–3 preceding standards, but increases markedly at 4 and above. These results suggest that Nd42AW may require a longer train of invariant sounds to establish regularity and encode deviance than N29AW.

There was no evidence of a systematic effect of the number of preceding standards on any components of LF oddball tone bursts (Figure not shown).

EPIDURAL ERP S TO LONG DURATION AND SHORT DURATION ODDBALL DEVIANTS IN AWAKE RATS

Unlike HF (or LF) DEVS, stimulus deviance for both LD and SD oddball DEVS can only be detected after 50 ms of a tone burst has elapsed. Therefore, one would not expect differences between oddball DEVS and STs or control DEVS prior to this point in time. As expected, LD oddball DEVS did not produce a larger N29AW than LD STs. However unexpectedly, P38AW appears larger, that is, more positive in LD oddball DEVS, particularly relative to LD STs (Figure 6A). At longer latencies, LD oddball DEVS showed a prolonged negative shift starting at 70 ms relative to LD ST ERPs. Similar late differences can be seen in the contrast between LD oddball DEVS and LD control DEVS (Figures 6A,B). SD oddball DEVS also exhibited differences relative to SD STs and consistent with the fact that information about duration deviance is only available after 50 ms has elapsed, these differences appear to onset at about 80 ms. However, in contrast to LD oddball DEVS, SD oddball DEVS were more positive than SD STs and SD control DEVS over longer latencies (Figures 6C,D). To capture these late effects, a 60-ms interval spanning longer latency displacements was extracted over a 100- to 160-ms and called here late DIFFAW2 to distinguish it from the late mean amplitude extracted for frequency oddball data. This measure was analyzed as well as N29AW and P38AW using repeated measures ANOVAs with two repeated measures factors, stimulus duration (long vs. short) and stimulus type (oddball DEV vs. ST or oddball DEV vs. control DEV).

There were no significant effects on N29AW amplitude for either oddball DEV vs. ST or control DEV contrasts (all p > 0.3). However P38AW exhibited a significant interaction between stimulus duration and type for the oddball DEV vs. ST contrast \( F(1, 6) = 7.25, p = 0.036 \) but not for the control DEV contrast \( p > 0.3 \). Simple effects contrast revealed that P38AW to the LD oddball DEV was significantly larger than the LD ST \( t = 3.98, p = 0.007 \); Figure 6E). We will return to this unexpected effect later. The equivalent contrast for SD stimuli was not significant.

Over the later latency window selected to capture the late negative displacement of oddball DEVS, late DIFFAW2 (an analysis breaking down this long interval to two smaller intervals...
FIGURE 6 | Epidural recorded ERPs in the awake rat to oddball deviant (oddball DEV), standard (ST), and control deviant (control DEV) in the duration conditions. (A) ERPs to long duration (LD) stimuli (150 ms) showing N29AW, P38AW, and late DIFF2AW2. LD oddball deviants (red) are negatively displaced over later latencies spanned by late DIFF2AW2 relative to both LD STs (blue) and LD control DEVs (black). P38 however is also larger to the oddball DEV, a problematic observation since the earliest the auditory system can detect that the DEV is longer is 50 ms (the duration of short standards in the LD DEV/SD ST oddball sequence). The horizontal bar indicates the latency window over which late DIFF2AW2 was measured. (B) MMN difference waves for LD stimuli: LD oddball DEV minus LD ST (blue), which can reflect both deviance detection and adaptation effects vs. difference waves derived using control deviants, LD oddball minus LD control DEV (black). (C) ERPs to short duration (SD) stimuli: N29AW and P38AW show no differences between the oddball DEV ERP (red) relative to the SD ST (blue) and relative to the control DEV (black). Over late latencies spanning late DIFF2AW2, the SD oddball DEV shows the opposite pattern to LD oddball DEVs in being positively displaced relative to SD ST and SD control DEV but not significantly so. (D) MMN difference waves for SD stimuli: SD oddball DEV minus SD ST (blue), and difference waves derived using control deviants, SD oddball DEV minus SD control DEV (black). (E) The mean amplitude (with SE) of N29AW, P38AW, and late DIFF2AW2 measures generated by long and short duration oddball DEVs (gray) and controls (white). (F) The mean amplitude (with SE) of N29AW, P38AW, and late DIFF2AW2 measures generated by long and short duration oddball DEVs (gray) and controls (white).

(100–130 and 130–160 ms) produced similar results), stimulus duration, and the interaction of stimulus duration × type either approached significance or were significant for both contrasts [oddball DEV vs. ST: duration $F(1, 6) = 4.40, p = 0.081$; interaction $F(1, 6) = 4.72, p = 0.073$; oddball DEV: duration $F(1, 6) = 9.12, p = 0.023$; interaction $F(1, 6) = 5.92, p = 0.022$]. The duration main effects were due to LD stimuli on average being more negative over this latency range relative to SD stimuli for both contrasts but more robustly so for the oddball DEV vs. control DEV contrast. Simple effects contrasts revealed...
that \( \text{DIFF}_{AW2} \) to the LD oddball DEV was significantly more negative than the LD control DEV (oddball DEV vs. control DEV: \( t(6) = -2.63, p = 0.039 \)). Equivalent simple effect contrasts for SD stimuli were not significant (Figure 6F). That is, LD oddball DEV ERPs (but not SD DEV ERPs) exhibited deviance detection in a late window extending from 100 to 160 ms. However, there was no evidence that this late negativity was sensitive to short-term stimulus history of background regularity as it did not show any systematic relationship with the number of preceding standard sounds. Therefore, evidence of MMN-like activity in ERPs to LD oddball deviants is not as strong as for HF oddball deviants.

We now turn to the results for \( P38_{AW} \) in the contrast between LD oddball DEV and LD ST. For both Duration MMN paradigms, \( P38_{AW} \) occurs before the offset of the shortest tone (i.e., 50 ms). It was expected therefore that \( P38_{AW} \) would be unaffected in both stimulus type contrasts. This however might not be the case if DEV and ST stimuli are presented in different contexts which indeed they are: LD DEVs are recorded in the ascending deviant oddball sequence whereas LD STs are recorded in the descending deviant oddball sequence. Therefore, we need to look more closely at DEV and ST ERPs from the same oddball sequence. For the LD DEV (150 ms) and SD ST (50 ms) from the same ascending DEV oddball sequence, the stimuli are presented pseudo randomly within the same block, and we see no difference in \( P38_{AW} \) amplitude between these stimuli as expected (Figure 7A; \( p > 0.05 \)). For the SD DEV vs. LD ST comparison from the reverse-standard–deviant oddball sequence, again the stimuli are presented pseudo randomly within the same block. Figure 7B suggests a difference in \( P38_{AW} \) amplitude, but it is not statistically significant (\( p = 0.20 \)). The problem arises when we compare the LD DEV to the LD ST. These stimuli are physically identical but are presented within different contexts (Figure 7C). The \( P38_{AW} \) to the LD ST is considerably smaller than that to the LD DEV (\( p = 0.007 \)). This difference is apparent in all seven rats. If we compare the SD DEV to the SD ST, then the problem is not so apparent and the difference is not significant although the amplitude of \( P38_{AW} \) measured relative to the preceding \( N29_{AW} \) is clearly reduced (Figure 7D). The implications are that \( P38_{AW} \) to both DEV and ST is consistently smaller during the LD ST/SD DEV oddball sequence than in the SD ST/LD DEV sequence. This conclusion is supported by the outcome of a two-way repeated

![FIGURE 7](image-url)
measures ANOVA on P38_{aw} amplitude with factors of oddball sequence (SD DEV/LD ST vs. LD DEV/SD ST) and stimulus type (DEV vs. ST). There is a significant effect of oddball sequence \([F(1, 6) = 7.25, p = 0.036]\), but no main effect of stimulus type and no interaction effect. We believe that these results indicate remarkable sensitivity of P38_{aw} to the predominant stimulus duration in oddball sequences – either (1) because of adaptation effects that are different for long and short stimuli or due to (2) the inter-stimulus interval before the deviant which is always 350 ms for the short DEV/long ST oddball sequence and 450 ms for the long DEV/short ST oddball sequence or (3) the duration of the preceding stimulus to the deviant which is always 150 ms for the short DEV/long ST oddball sequence and 50 ms for the long DEV/short ST oddball sequence.

**Epidural ERPs to Oddball Deviants in Anesthetized Rats**

Despite the relatively noisy recordings and considerable instability in pre-stimulus intervals, ERPs recorded under anesthesia for the four oddball DEVs (HF, LF, LD, and SD) showed consistent displacements relative to their respective STs and control DEV ERPs. In each instance, the oddball DEV ERP exhibited a prolonged positive displacement relative to ST and control DEV ERPs (Figures 8A–D) with an onset latency prior to N67_{an} and persisted until approximately 120 ms post-stimulus (see Figure 8E) for average over all four stimulus types: HF, LF, LD, and SD). These effects are superimposed on offset potentials evident in most waveforms. Therefore, the same measurement windows were used for all four oddball DEV conditions: N67_{an} and two later windows spanning 70–100 and 100–130 ms, which will be referred to here as late DIFF_{an1} and late DIFF_{an2}. Each of these measures was analyzed using ANOVAs with two repeated measures factors, deviant type with four levels (HF, LF, LD, and SD) and stimulus type with two levels (oddball DEV vs. ST or oddball DEV vs. control DEV).

There were no significant main effects or interactions involving deviant type on any ERP measure indicative of the insensitivity of onset ERPs under anesthesia to stimulus parameters. However, the oddball DEV exhibited a significant positive displacement relative to the ST over both N67_{an} \([F(1, 6) = 7.25, p = 0.036]\) and the late DIFF_{an1} \([F(1, 6) = 7.01, p = 0.038; Figure 8F]\). Both measures showed a similar pattern when the oddball DEV was compared to the control DEV [N67_{an}: \(F(1, 6) = 6.29, p = 0.046\); late DIFF_{an1}: \(F(1, 6) = 5.78, p = 0.053; Figure 8F\)]. Neither contrast was significant over the later interval (late DIFF_{an2}). Although these results should be treated cautiously given the data quality, they nonetheless suggest that in the anesthetized animal, MMN-like potentials take the form of a positive displacement of the deviant ERP.

**Discussion**

This study sought evidence of MMN-like activity in epidural potentials in awake and anesthetized rats to HF and LF and LD and SD deviant sounds. In order to determine whether MMN-like activity reflects deviance detection relative to background regularity or differential adaptation due to the rarity of deviants, epidural ERPs to deviant oddball sounds were compared not only with ERPs to a common standard with the same physical features to the deviant but also with ERPs to the same tone as the many-standards control deviant. The main findings were: (a) epidural ERPs in the awake animal showed evidence of deviance detection to both HF and LD deviants. MMN-like activity was evident as negative displacements of the oddball deviant ERP relative to ERPs to a common standard and a deviant with many standards. (b) The awake MMN-like response to HF deviants was also sensitive to local temporal context of preceding stimulus regularity: it increased with the number of preceding standards prior to the deviant sound. The MMN-like response to LD deviants was not sensitive to local stimulus history. (c) LF deviants and SD deviants did not elicit consistent MMN-like responses in the awake rat. (d) Anesthesia resulted in positive displacements of the oddball deviant ERP relative to ERPs to the standard with the same physical features and the many-standards control deviant, that is, a polarity reversal of the MMN-like responses seen in the awake rat.

**The Effects of Deviant Features on Epidural ERP Components and MMN-Like Responses**

Previous reports utilizing epidural recordings in the rat also claim to have found evidence of MMN-like activity to simple invariance frequency and duration deviants (Table 1). We used frequencies similar to the 2000- and 2500-Hz stimuli used in the Tikhon- ravov et al. (2008, 2010) reports and therefore the lack of MMN to LF deviants might appear inconsistent with these reports, but neither analyzed LF and HF deviants separately. The lack of MMN-like activity to LF deviants in our data could be attributed to the 2500-Hz tone being less optimal for the Wistar rat. This was evident in the smaller amplitude of two major ERP components, N29 and N90, to any tone burst of 3000 Hz or less in the many-standards frequency control sequence (see Figures 2A, B) and is consistent with limited data available on the rat frequency audiogram (Jamison, 1951; Gourevitch, 1965; Mazurek et al., 2010). However, Astikainen et al. (2011) have also recently reported MMN-like responses to ascending (high) frequency deviants but not to descending (low) deviants. The authors draw attention to similar asymmetries in MMN (Peter et al., 2010) and auditory discrimination thresholds (Kishon-Rabin et al., 2004) in humans.

Our duration deviant data are comparable, in one respect, with the only published paper reporting duration MMN data in rats (Roger et al., 2009) in that MMN-like activity appeared as a negative displacement of deviant relative to the standard ERP, although in our study only the LD deviant showed significant evidence of an MMN-like response. However, some caution is warranted in interpreting these data as evidence of MMN-like activity, since the late negative displacements in deviant ERPs were insensitive to the degree of preceding stimulus regularity. We were unable to replicate the Roger et al. (2009) duration decrement findings despite the design of our duration decrement oddball sequence being similar to the condition which elicited the largest MMN-like response in Roger et al. (2009). However, the asymmetric findings in our data once again have parallels in the human MMN and auditory perception literature. MMN to duration decrements are smaller than duration increments (Catt et al., 1995), even with equivalent physical differences between deviants and standards. Analogous asymmetries have also been observed in psychoacoustical studies in humans (Cusack and Carlyon, 2003).
FIGURE 8 | Epidural recorded ERPs in the anesthetized rat to oddball deviant (oddball DEV), standard (ST) and control deviant (control DEV) for both the frequency and duration oddball sequences. (A,B) ERPs to oddball DEV (red), ST (blue), and control DEV (black) for high frequency (HF) and low frequency (LF) stimuli respectively. (C,D) ERPs to oddball DEV (red), ST (blue), and control DEV (black) for long duration (LD) and short duration (SD) stimuli respectively. All four stimuli show a similar pattern (unlike the awake state): oddball DEVs show a positive shift relative to STs and control DEVs. (E) ERPs obtained by averaging over all stimulus conditions to produce averaged oddball DEV, ST, and control DEV ERPs providing a depiction of the positive displacement of oddball DEVs relative to STs and control DEVs. (F) Mean amplitudes (with SEs) of N67_an, late DIFF_an1, and late DIFF_an2 generated by oddball DEVs (red), STs (blue) and control DEVs (black) showing that N67_an and late DIFF_an1 are both more positive than STs ($p = 0.046$) and control DEVs ($p = 0.053$).
DEVIANCE DETECTION IN RAT EPIDURAL RECORDINGS: THE OPTIMAL CONTROL CONDITION

As noted in the introduction, previous reports of MMN-like activity reflecting deviance detection in rat epidural potentials (Ruu suvırtıa et al., 1998; Tıkkıonı ravı et al., 2008, 2010) used a control condition in which the deviant alone was presented without standards at the same interstimulus interval as the oddball sequence. The rationale is that if the MMN-like activity is not present in the deviant-alone ERP, the MMN-like activity in the oddball deviant cannot be attributed to differences in adaptation, but is reliant on the presence of stimulus regularity established by the presence of standards. However, auditory cortex neurons have complex temporal dynamics, so that stimulus sequences that differ with respect to interstimulus intervals may engage very different mechanisms (Nelken and Ulanovsky, 2007). Consensus is emerging that the deviant with many different standards paradigm is the best control for differential adaptation effects, stimulus features and background context regularity (Nelken and Ulanovsky, 2007). Our data demonstrate that epidural potentials show evidence of deviance detection in the awake rat using this control for the HF deviant and for the LD deviant, and in the anesthetized rat when averaged over the four deviants (HF, LF, LD, and SD). Interestingly, our data also show that in general there were only minor differences between MMN-like activity extracted using the many-standards control vs. the common standard (with the same physical attributes as the deviant). Evidence of deviance detection has also recently been reported in epidural potentials of anesthetized rats using the many-standards control (Astikainen et al., 2011). Further, Taaseh et al. (2011) concluded that there was evidence of deviance detection in MUA and eLFP responses of anesthetized rats based on data showing that observed MUA and eLFP responses to the deviant were larger than predicted responses derived from a model of SSA that included only adaptation of responses in narrow frequency channels. In contrast, other studies using MUA and eLFP recordings in rat AC concluded that there was no evidence for deviance detection (von der Behrens et al., 2009; Farley et al., 2010). These inconsistencies may be due to a variety of methodological differences between the respective studies.

Some caveats are necessary in relation to the design of the many-standards control. In the control sequence there were five different tones. If the control DEV was positioned as either the upper or lower extreme within this set, then it is possible that they may be perceived as deviant compared to the non-extreme stimuli. This extreme sub-standard effect has been noted, particularly for duration (Jacobsen and Schröger, 2003). To avoid this possibility, in this study, the equivalent of the frequency deviants (HF and LF) were positioned either side of the middle frequency in the range such that there was an intervening frequency between them (see Figure 1A). The problem with this design is that it is possible that the smaller N29 in the HF control deviant (Figure 4A) could be accounted for by greater adaptation of exogenous N29 generators caused by partly overlapping frequency-specific neural populations responding to tones adjacent to HF. However, it is unlikely that similar caveats apply to the later negativities, Nd42aw and the late DIFFaw – they appear to be a separate non-exogenous components associated with deviance detection and in the case of Nd42aw in particular, behave similarly to the human MMN [i.e., the ERPs to the oddball deviant is more negative than the ERPs to the control deviant (Figure 4F) and the amplitude of the negative displacement is sensitive to the local probability of the oddball deviant (Figure 5C)].

ANESTHESIA EFFECTS

Anesthesia resulted in a polarity reversal of MMN-like potentials, that is, a positive displacement, a finding that is consistent with most previous findings in anesthetized rats except for Ruusuvırtıa et al. (2007) and Eriksson and Villa, 2005; see Table 1). Previously, N-methyl-D-aspartate receptor antagonists have been suggested to affect MMN-like activity in animals (Javitt et al., 1996; Tıkkıonı ravı et al., 2008, 2010) and the absence of MMN-like activity in the anesthetized rats in Eriksson and Villa (2005) may be due to the use of ketamine. In the current study, anesthesia also resulted in marked reductions in ERP component amplitudes to tone bursts, a loss of frequency sensitivity of ERP component amplitudes in the frequency control sequence and the appearance of offset potentials in the duration control sequence which were essentially absent in the awake state. In general, the activity of AC neurons tends to be reduced by general anesthetics and characterized by more phasic responses and reduced sustained firing relative to the awake state (Zurita et al., 1994). Barbiturates in particular may both depress excitation and enhance inhibition (Pocock and Richards, 1993). However, the extent and nature of the effect on AC neurons varies with different anesthetics (Moshıtıch et al., 2006). There are no data to our knowledge on the combined effect of two anesthetics used in this report, fentanyl, a mu-opioid receptor agonist, and medetomidine, a selective alpha 2 adrenoceptor. The presence of offset responses under anesthesia in our data point to potentiation of inhibition as larger offset responses in the rat are associated with greater inhibitory rebound following cessation of a stimulus (Takahashi et al., 2004). Alterations in the relative balance of excitation and inhibition under anesthesia (Wehr and Zador, 2003; Rennaker et al., 2007) may also explain not only the loss of sensitivity of early ERP components to tone burst frequency but also the polarity reversal of MMN-like response. In humans, widespread cortical surface negativities have been associated with cortical excitability (Birbaumer et al., 1990), whereas cortical surface positivities are associated with cortical disfacilitation or inhibition (Shupp et al., 1994). Further research is required to understand the cortical circuitry producing either negative or positive displacements.

IMPLICATIONS FOR FUTURE TRANSLATIONAL RESEARCH

Although it has been claimed in the past that MMN potentials in humans and rodents are homologous (Bıckel and Javitt, 2009), such a claim could be seen as premature as attempts to demonstrate a deviance detection MMN in rats to date have resulted in patterns that have been portrayed as “weak or ambiguous” (von der Behrens et al., 2009, p. 13837). However, if the effects observed here for HF deviants are replicated with an improved design, it becomes feasible to exploit MMN as an endophenotype in translational research aimed at testing a range of animal models of schizophrenia, and to assess the likely efficacy of new compounds (Luck et al., 2011).
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